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A Subnanosecond Pulsed Electric Field System for Studying Cells Electroporation

Njomza Ibrahim, *Graduate Student Member, IEEE*, Leslie Vallet, Franck M. Andre, *Member, IEEE*,

Laurent Ariztia, Marc Rivaletto¹, Antoine Silvestre de Ferron¹, Bucur Mircea Novac¹, *Senior Member, IEEE*, Lluís M. Mir, and Laurent Pécastaing¹, *Senior Member, IEEE*

Abstract—This article presents an experimental arrangement which, using 3-D numerical modeling, aims to study biomedical effects using subnanosecond pulsed electric fields (PEFs). As part of a major effort into developing contactless technology, the final aim of this study is to determine conditions of the applied PEFs (number of pulses, strength, pulse repetition frequency) able to produce electroporation. The arrangement uses a pulsed power generator producing voltage impulses with an amplitude of up to 20 kV on a 50-Ω matched load, with a rise time of 100 ps and a duration of 600 ps. During the preliminary study reported here, samples containing *E. Coli* were exposed to PEFs in a 4-mm standard electroporation cuvette, allowing the application of a peak electric field strength of up to 60 kV/cm. The studies were facilitated by detailed 3-D electromagnetic modeling of the electric field distribution generated by voltage impulses inside the system. Due to the nature of tests, the numerical analysis played an essential role in the interpretation of results. Preliminary biological results reported in this study are very encouraging, showing that trains of 5000 to 50000 pulses applied at a pulsed repetition frequency of 200 Hz (maximum PRF) can efficiently induce *E. Coli* electroporation.

Index Terms—Biological cells, electroporation, pulsed electric fields (PEFs), pulsed power, subnanosecond pulses.

I. INTRODUCTION

THE use of narrow-band electromagnetic fields for application to medicine and biology has received significant attention by the scientific community over the last few decades [1]. Electroporation (electric pore formation) is a phenomenon which increases the permeability of the cell membrane when exposed to pulsed electric fields (PEFs) of high intensity

and short duration. The pore formation generates openings in the cell membrane, allowing for the transfer of therapeutic molecules across the cell membrane [2], [3]. Thus, the electroporation phenomenon contributes to the efficiency of electrochemotherapy, when used with drugs [4] and electrogenotherapy, when used with DNA plasmids [5].

PEFs can cause reversible electroporation, i.e., a temporary permeabilization of the cell membrane [6], but they can also produce irreversible electroporation, i.e., cell death, for eradicating cancerous or other unwanted cells [7].

There are basically two types of PEF techniques applied *in vivo*: *invasive*, where metallic pairs of penetrating electrodes are used to apply the electric field and *noninvasive*, where the electric field is generated through electrodes brought in contact with the skin, without penetration of the body. In addition, the *contactless* term refers here to the approach dealing with the generation of electric fields remotely from the metallic structure of a PEF source (*antenna*).

The *electrode-based contact* technology is already successfully applied in the treatment of various cancers including, but not limited to, kidney, liver, lung, and bone cancers [8]. Pulses having hundreds of ns duration applied for cancer treatment are still under clinical trials and as such are not part of regular treatments. PEFs of about 100 μs are widely used, depending on the type and the evolution of cancer while ms pulses are not used for cancer treatment. The outcome effect depends not only on the magnitude and duration of the PEFs delivered, but also on the pulse repetition frequency (PRF) and on the characteristics of the tissue, in particular, its conductivity. Irreversible electroporation using microsecond very high intensity PEFs in the tissues is widely considered in many hospitals. An advantage of this technique is that the thermal effects are considerably lower, when compared to other ablation techniques [9]. Cancer treatment techniques, which include but are not limited to chemotherapy and surgery, are unfortunately accompanied by adverse side effects imposed on the patient [10], [11]. The future of the PEF-based cancer treatment techniques is therefore closely related to the identification of new ways to avoid the challenges imposed by the existing *invasive* surgical procedures. The pathway toward a *contactless* technology, a nonsurgical procedure, which aims at overcoming some of the issues mentioned above, was studied in very few research laboratories worldwide. The reason for the very limited number of publications published in this domain is perhaps due to the fact that, depending on their output voltage, the highly specialized HV subnanosecond pulsed

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Njomza Ibrahim, Laurent Ariztia, Marc Rivaletto, Antoine Silvestre de Ferron, and Laurent Pécastaing are with the Laboratoire des Sciences de l'Ingénieur Appliquées à la Mécanique et au Génie Électrique – Fédération IPRA, Université de Pau et des Pays de l'Adour/E2S UPPA, 64000 Pau, France (e-mail: laurent.pecastaing@univ-pau.fr).

Leslie Vallet, Franck M. Andre, and Lluís M. Mir are with Université Paris-Saclay, Institut Gustave Roussy, CNRS, Metabolic and Systemic Aspects of Oncogenesis (METSYS), 94805 Villejuif, France (e-mail: luis.mir@cns.fr).

Bucur Mircea Novac is with the Wolfson School of Mechanical, Electrical and Manufacturing Engineering, Loughborough University, Loughborough LE11 3TU, U.K., and also with the Laboratoire des Sciences de l'Ingénieur Appliquées à la Mécanique et au Génie Électrique – Fédération IPRA, Université de Pau et des Pays de l'Adour/E2S UPPA, 64000 Pau, France (e-mail: b.m.novac@lboro.ac.uk).

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power generators required are either extremely expensive or only available at military related research centers. Even more difficult, the focusing of electromagnetic radiation with very high precision in a volume around 1 cm^3 , or preferably even lower, is possible only using highly sophisticated impulse antenna techniques.

Two possible solutions were suggested theoretically by Carl Baum, as part of a major research effort undertaken by the Frank Reidy Research Center for Bioelectrics at Old Dominion University (USA): an impulse radiating antenna (IRA) operated in air [12], [13], in combination with a complex many layer dielectric lens [14] and another prolate-spheroidal reflector, operated underwater [15]. More recently, at the same research center, a dielectric rod antenna was also suggested as a candidate for generating subnanosecond PEFs for the stimulation of neurological tissue [16]. All the three techniques have been theoretically investigated using CST software [15]–[17], with detailed numerical studies being reported. In contrast, very limited experimental work has been published, and only using rather low voltage subnanosecond pulsed power generators, with the resulting PEFs having extremely low peak values when compared with the values required for electroporation [18]–[20], the latter work representing an effort made at University of Limoges (France). For stimulating deep inside a tissue, say at 8 cm [17] using intense PEFs of some tens of kV/cm, published work suggest a subnanosecond pulsed power generator with a peak output voltage in excess of 250 kV is required [17]. Such a generator is technically extremely challenging.

Another aspect is that when using such innovative *contactless* delivery systems, the characteristics of the subnanosecond PEFs are different when compared with those of the existing PEF processing. A logical step is therefore to understand their action on cells by firstly using standard electrode-based PEFs driven by subnanosecond pulsed power generators. Results published by the Old Dominion team and also by a research group at Chongqing University (China), demonstrated that subnanosecond PEFs can indeed produce: permeabilization [21] followed by the transfer of molecules inside the cell [22], cell stimulation with calcium mobilization (through VGCCs activation) [23], and apoptosis (cell death) [24]–[27]. The main issue with these results however is that they suggest a very low efficiency of processing for a PEF having a relatively low peak value, say around 25 kV/cm, as it is expected to be generated in a deep tissue by a *contactless* reflector-based system. Under such conditions, to obtain the effect on a significant percentage of cells, it was necessary to apply an extremely large number of pulses, of the order of a few millions [22].

The development of *contactless* PEF technologies has been a major research theme in the long history of an ongoing collaboration between Pau University and Loughborough University and two major works have been already published discussing a novel technique for food processing [28] and a subnanosecond driven prolate antenna operated underwater [29]. The latter work reports the first practical demonstration of generating underwater a peak PEF of 50 kV/cm at 8 cm away from any metallic structure,

i.e., fulfilling the conditions required for *contactless* deep tissue permeabilization [17].

The arrangement reported here is using a standard electrode-based approach. In the preliminary phase of this study, it was decided to apply PEFs on the *E. Coli* DH5 α bacteria, which are very small cells with a diameter in the range of $1 \mu\text{m}$.

First, the pulsed power generator will be introduced, together with its corresponding diagnostics.

Second, a detailed 3-D model is presented, based on the CST Microwave Studio, a 3-D finite integral time-domain (FITD) electromagnetic simulation software [30]. As the direct measurement of the PEF generated inside a cuvette containing the cell culture is technically challenging, a comprehensive 3-D modeling and numerical electromagnetic analysis were essential during the experimental studies.

Third, we report encouraging preliminary results that demonstrate that a high percentage of permeabilized bacteria can be achieved using the described arrangement.

This conclusion ends with conclusions and a brief presentation of the way ahead.

II. EXPERIMENTAL ARRANGEMENT

For the present studies, a pulsed power generator similar to that described in [31] was adapted for use as a subnanosecond transient source capable of producing high voltage pulses with an amplitude of up to 20 kV and having a 100-ps rise time on a 50- Ω matched load, with a duration of about 600 ps. The generator is connected to the PEF processing load through a 2.5-m-long RG214-U type coaxial 50- Ω cable, having an insulator made of polyethylene with relative permittivity of 2.26. A simplified scheme of the pulsed power arrangement is shown in Fig. 1. The generator is constructed as a fast pulse forming line, with the closing switch operated under high-pressure hydrogen. To obtain a 20-kV peak voltage output, the product of the hydrogen pressure and the gap distance of the electrode system was held to 22 bar \cdot mm. This value was then adjusted to obtain other values for the output peak voltage. The output voltage is measured using a capacitive voltage divider, the main voltage probe, attached to the RG214-U coaxial cable [Fig. 1(b)]. The transmission coefficient for this probe is equal to -46 dB all over the frequency bandwidth and the reflection coefficient is lower than -12 dB while the cut-off frequency is close to 6 GHz.

The PEF processing load connected at the end of the RG214-U coaxial cable [Fig. 1(b)] consists of two parallel-plate electrodes made of copper. The distance between copper electrodes is fixed to 12 mm to allow mounting between them a standard electroporation cuvette, having a gap distance of 4 mm between its internal aluminum electrodes. The volume of the sample which contains the deionized water to be tested was kept at 100 μL for two reasons. First, to obtain the desired PEF in water in terms of amplitude, rise time, and duration and second to reduce the impedance mismatch. To avoid any possible electric breakdown, the upper part of the cuvette was additionally filled with 1.6 mL of paraffin oil, having a relative permittivity 2.33. It is important

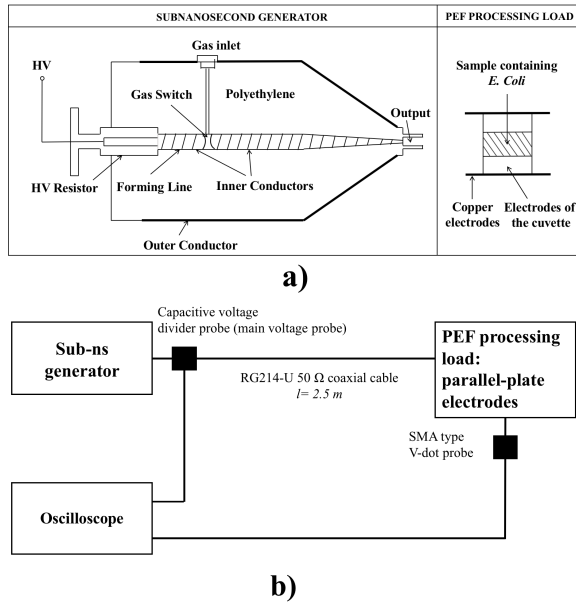


Fig. 1. Pulsed power arrangement for subnanosecond PEF. (a) Subnanosecond generator (adapted after [31]) and PEF processing load. (b) Overall schematic.



Fig. 2. Experimental arrangement for subnanosecond PEF processing. The numbers 1–6 represent the generator (1), capacitive voltage divider (main voltage probe) (2), RG214-U 50 Ω coaxial cable (3), two parallel-plate electrodes (4), 4-mm electroperoration cuvette (5), and SMA-type V-dot probe (6).

to note that the dielectric strength of the present experimental arrangement, when subnanosecond electric pulses are applied, is much higher compared to cases when 50-Hz ac, microsecond or longer duration pulses are applied. The complete experimental configuration is presented in Fig. 2. An SMA-type V-dot probe is mounted just a few millimeters below the cuvette with the connector's body attached to the ground plate electrode. This probe is used to control the voltage across the cuvette, with the electric field in the cuvette obtained using the numerical technique described in the following.

III. NUMERICAL TECHNIQUES

A detailed 3-D modeling and EM analysis were carried out for the PEF system. To shorten the time required for numerical analysis of the 50- Ω (RG214-U) coaxial cable, only a length of 101 mm was considered, corresponding to a propagation time of 0.5 ns. The 3-D CST model of the

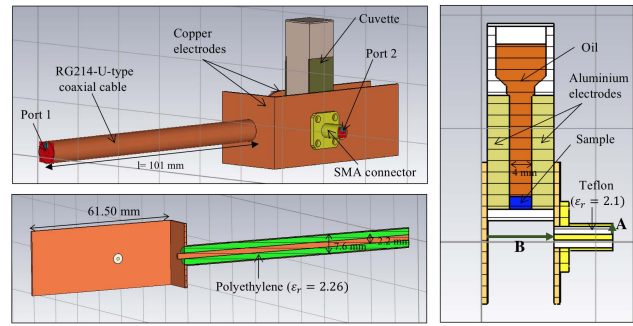


Fig. 3. Complete CST model for the PEF processing chamber, including the RG214-U coaxial cable, the two parallel-plate copper electrodes with the SMA-type V-dot probe attached and the electroperoration cuvette, with two compartments filled with paraffin oil and water sample, which may contain bacteria. The two CST ports are highlighted.

PEF processing load is presented in Fig. 3. The presence of bacteria in the water contained inside the cuvette was not taken into consideration in the CST simulation, as measurements of electrical permittivity and the real signals recorded from the SMA-type V-dot probe, both demonstrated the bacteria do not introduce a significant difference. To analyze the impedance profile along the coaxial cable and in the PEF processing load and to better understand its behavior due to the presence of the electroperoration cuvette, we have numerically performed the time domain reflectometry (TDR) task in CST. The TDR was evaluated based on the reflected signals using the integrated Gaussian signal shown in Fig. 4, with a rise time of 219 ps and a frequency bandwidth of 4 GHz, following the CST manual formula [30]:

$$Z(t) = Z_0 \frac{\int_0^\infty i(\tau) d\tau + \int_0^t o(\tau) d\tau}{\int_0^\infty i(\tau) d\tau - \int_0^t o(\tau) d\tau} \quad (1)$$

where Z_0 is the characteristic impedance of the coaxial cable, i.e., 50 Ω , $i(t)$ is the incident signal at CST Port 1 (Fig. 3) and $o(t)$ is the reflected signal at the same port. Fig. 5 shows the impedance is 50 Ω along the coaxial cable and then at 1 ns, which corresponds to the return end of the coaxial cable, the impedance starts to increase to a value of 70 Ω . This effect is due to the *mismatch* between the coaxial cable and the PEF processing load. At around 1.2 ns the impedance starts to decrease and at 1.4 ns attains a minimum value of 32 Ω . This impedance decrease is due to the cuvette, which is placed at a distance of 121 mm from the coaxial cable input (Port 1). At around 1.8 ns the impedance again increases rapidly this time due to the open end of the PEF load. Both incident and reflected signals at Port 1 were carefully analyzed to observe the impedance distribution within the electric assembly. In addition, the estimation of the TDR allows us to have a representation of the time variation of the PEF processing load reflection coefficient (Fig. 6).

The electric field distribution inside the cuvette was studied using the CST Electrostatics solver. The cuvette behaves like a collection of two parallel plate capacitors mounted in parallel, one containing paraffin oil and the other water. Because of this, the electric field strength is the same in the two media, but the displacement fields are different. CST calculations indicate for

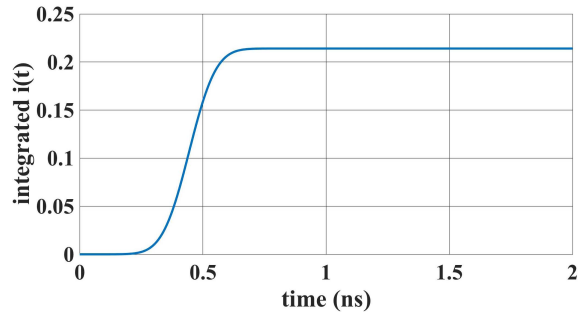


Fig. 4. Integrated Gaussian signal used to perform the TDR task.

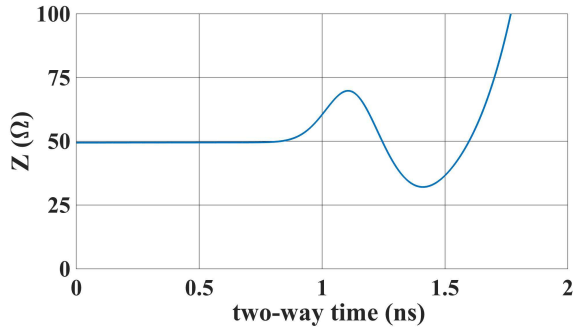


Fig. 5. Impedance profile along the cable and the processing load.

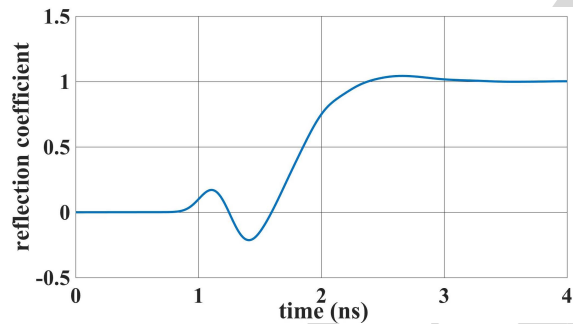


Fig. 6. Time variation of the reflection coefficient for the PEF processing load.

246 the cuvette a total equivalent capacitance of 5.95 pF, a value
 247 allowing voltage pulses having about 258-ps rise time to be
 248 delivered to the PEF processing load.

249 IV. DETERMINATION OF THE TIME VARIATION OF THE 250 ELECTRIC FIELD IN THE PROCESSED WATER SAMPLE

251 Because of the very small size of the water sample to be
 252 processed, there are no available techniques that can be used
 253 to directly measure the electric field generated inside. The
 254 only way to determine this essential parameter, which allows
 255 the correct interpretation of the biological results, is to use
 256 a combination of numerical modeling predictions and experi-
 257 mental evidence. Firstly, a detailed 3-D CST electromagnetic
 258 analysis of the load was carried out, including the SMA-type
 259 V-dot probe mounted near the cuvette (Fig. 7). The input
 260 signal applied to the processing load (see Fig. 8) was accu-
 261 rately measured using the main voltage probe attached to the
 262 RG214-U coaxial cable described above. This experimentally

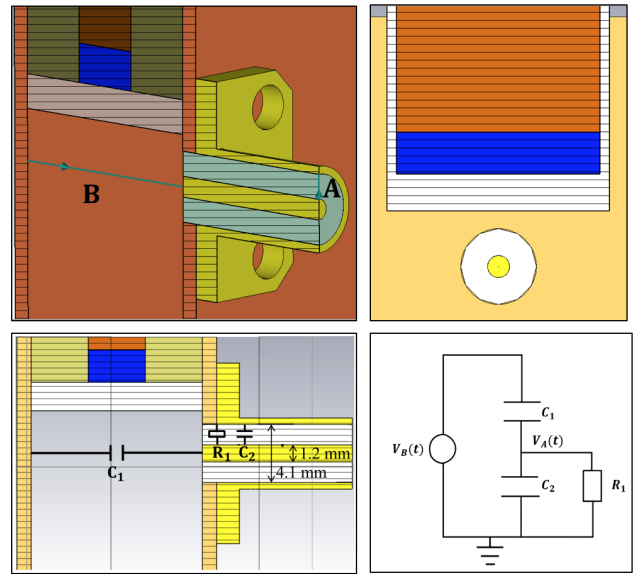


Fig. 7. Top: V-dot probe mounted inside the PEF load, near the cuvette containing the water to be processed. Bottom: its corresponding equivalent electric scheme, following that described in [32] and [33].

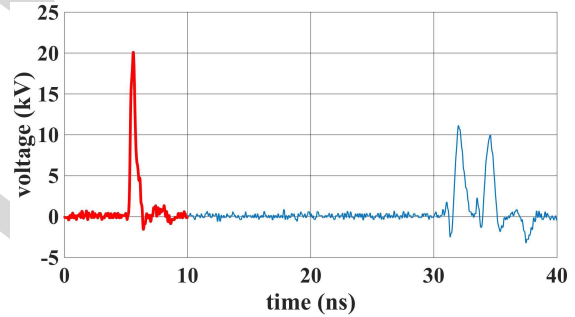


Fig. 8. Complete signal recorded from the main voltage probe considering the total length of 2.5 m for the RG214-U coaxial cable. The first 10 ns of the experimental voltage signal (highlighted) are used as CST input data.

obtained voltage signal, with a rise time of about 258 ps and
 FWHM about 434 ps, was then used as an input (or excitation
 signal) for the CST Port 1 situated at the coaxial cable input
 (Fig. 3). To check the model, the predicted reflected signal was
 then successfully compared with the experimentally recorded
 reflected signal (see Fig. 9). To allow this comparison, the time
 delay of the signal due to the 2.5-m coaxial cable (see Fig. 8)
 was adjusted to the corresponding shorter time delay of only
 101-mm length of cable considered by the CST model (see
 Fig. 9). A second comparison between CST predictions and the
 experimental data was performed for the CST Port 2 situated
 at the V-dot probe output (Fig. 3). Fig. 10 demonstrates the
 very good similarity between the predicted and the measured
 signal.

The above presented preliminary work had two important
 consequences.

- 1) Following [32], the SMA-type V-dot probe could be calibrated, with the voltage $V(t)$ calculated from the

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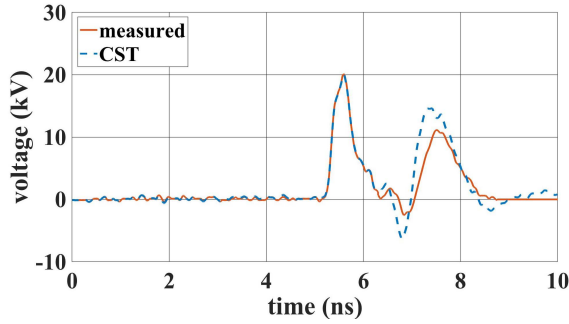


Fig. 9. Full line: experimental signal obtained from the main voltage probe. Dotted line: CST prediction for the voltage at Port 1.

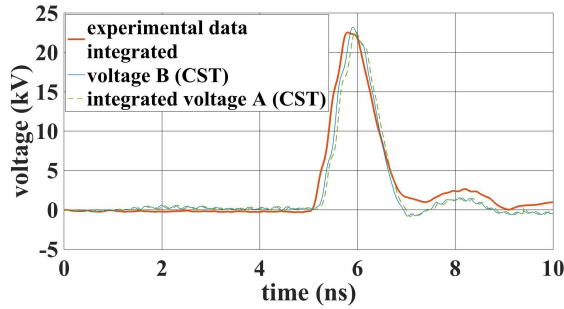


Fig. 10. Second comparison between CST model and experimental data. Thick line: time dependence of the integrated voltage signal from V-dot probe. Thin line: CST prediction obtained from a virtual voltage probe placed at location B. Dotted line: integrated voltage signal output from Port 2 placed at location A. The location of both A and B is presented in Fig. 7. The two CST generated traces are practically indistinguishable demonstrating that, due to the favorable electric field distribution, the SMA probe acts indeed as a V-dot probe [33].

probe output voltage signal $V_{\text{signal}}(t)$ as:

$$V(t) = \frac{1}{\tau} \int_0^t V_{\text{signal}}(t) dt \quad (2)$$

where $\tau = Z_0 \cdot C_1$, with $Z_0 = 50 \Omega$ being the impedance of the cable connecting the probe to oscilloscope and $C_1 = 2.9 \text{ fF}$ the probe coupling capacitance [32], [33], as shown in Fig. 7 was obtained using CST calculations.

- 2) The following procedure was established. During testing, the electric field generated inside the water sample is calculated by CST, using an input voltage Port 1 based on the experimentally measured input voltage signal. However, as a precaution, the CST predictions for Port 2 are always checked against the experimental signal generated by the V-dot probe housed inside the load. If the two are identical, the CST results are most likely correct. If the two are different, a possible explanation could be that electric breakdowns are present inside the processing load.

As an example, Fig. 11 presents the calculated time variation of the electric field strength inside the water sample for the experimental conditions of Fig. 9, i.e., when the peak transient voltage input reaches a peak of 20 kV. The corresponding peak electric field strength reaches 58 kV/cm, with a rise time of 303 ps and an FWHM of 773 ps. At this moment, the corresponding electric field distribution inside the processing load

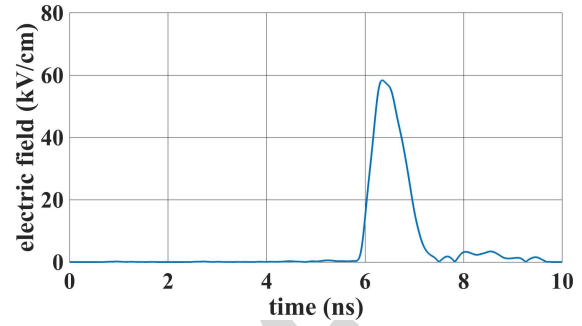


Fig. 11. PEF parameters generated inside the cuvette water sample, for the input conditions of Fig. 9. The peak electric field strength is reaching 58 kV/cm, with a rise time of 303 ps and a FWHM of 773 ps.

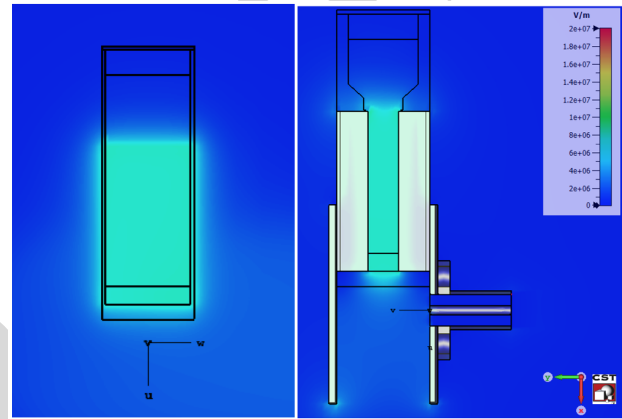


Fig. 12. Electric field distribution inside the processing load at the moment the peak field of 58 kV/cm is generated inside the cuvette water sample (see Fig. 11).

is shown in Fig. 12. It is important to note two essential characteristics: 1) the electric field is mainly concentrated inside the cuvette and 2) inside the cuvette the electric field is highly homogeneous, allowing a simple interpretation of the results obtained after PEF processing.

When performing a large number of tests at a high PRF, one important question is related to the possible temperature increase of the water sample. The variation of temperature ΔT during N consecutive shots is given by

$$\Delta T = \frac{W}{m C_p} N \quad (3)$$

where W is energy deposited in the water during one shot, $m \approx 100 \text{ mg}$ is the mass of the water sample and $C_p = 4188 \text{ J/kg/K}$ is the constant-pressure heat capacity of water at $25 \text{ }^\circ\text{C}$ [34]. The energy is calculated as

$$W = R \int_0^t I^2(t') dt' \quad (4)$$

where R is the water sample resistance while the current integral was performed using data from a CST virtual current sensor. As the water sample has a conductivity of about $\sigma = 300 \mu\text{S/m}$ and a relative permittivity $\epsilon_r = 78.4$ at $25 \text{ }^\circ\text{C}$ [35], the time constant $\epsilon_0 \epsilon_r / \sigma = 140 \mu\text{s}$ is much larger than the pulse duration ($\approx 2 \text{ ns}$) and therefore the conduction

326 current can safely be ignored. In such conditions the water
327 series equivalent resistance can be estimated as

$$328 \quad R = \frac{\tan \delta}{2\pi f C_w} = 1.28 \, \Omega \quad (5)$$

329 where $\tan \delta = 0.005$ [35] is the water loss tangent at a
330 frequency f estimated as $f = 0.35/t_{\text{rise}} = 1.35$ GHz, where
331 $t_{\text{rise}} = 258$ ps is the rise time of the impulse. The equivalent
332 capacitance C_w of the water sample was calculated using CST
333 as $C_w = 4.6$ pF. As a typical result, after applying $N = 50\,000$
334 consecutive shots, the estimated water sample temperature
335 increase is only $\Delta T = 0.00615^\circ\text{C}$ and therefore negligible.

336 V. BIOLOGICAL TECHNIQUES

337 *E. Coli* DH5 α were purchased from Invitrogen
338 (Courtaboeuf, France). Cultures used for experiments
339 were grown from 80 μL of bacterial stock solution (saturated
340 bacterial broth mixed with glycerol in (1:1) ratio stored at
341 -80°C) added to 8 mL of Luria Bertani (LB) medium
342 (Invitrogen LB broth base Lennox L) and incubated at 37°C
343 under constant orbital shaking at 220 r/min for 8 h over day,
344 corresponding to an endpoint OD600 of approximately 0.9.
345 Cultures were then placed at 4°C overnight until used for
346 experiments on the next day. *E. Coli* permeabilization was
347 assessed using a cell-impermeant fluorescent nucleic acid
348 stain entering only permeabilized bacteria, the YO-PRO-1
349 iodide ($\lambda_{\text{ex}} 491/\lambda_{\text{em}} 509$) (Invitrogen). *E. Coli* gating in flow
350 cytometry was validated using a cell-permeant fluorescent
351 nucleic acid stain entering all bacteria, permeabilized or not,
352 the SYTO 9 ($\lambda_{\text{ex}} 485/\lambda_{\text{em}} 498$) (Invitrogen). Prior to PEF
353 exposure, bacteria were centrifuged at $2000 \times g$ for 20 min,
354 the supernatant was discarded and the bacterial pellet was
355 resuspended in the same volume of sterile deionized water
356 (same bacterial concentration than mother culture). Then,
357 either YO-PRO-1 iodide or SYTO 9 was added (working
358 concentrations of 30 and 50 μM , respectively). A volume
359 of 100 μL of bacterial suspension with marker (YO-PRO-1
360 iodide or SYTO 9) was then placed in a 4-mm wide gap
361 commercial electroporation cuvette (Cell Projects Ltd, Kent,
362 U.K.) and covered with 1.6 mL of insulating paraffin oil
363 in order to prevent arcing between electrodes during PEF
364 exposure. Then, pulses were delivered at room temperature
365 by installing the electroporation cuvette in the applicator
366 presented in Fig. 3. Controls were sham exposures for which
367 all the steps of the exposure protocol were followed, except
368 for the PEF delivery. 5 min after PEF exposure, a volume
369 of 50 μL of the bacterial suspension was collected from
370 the cuvette and mixed with 50 μL of sterile deionized
371 water. On average 30 min after PEF exposure, and prior
372 to flow cytometry analyses, this bacterial suspension was

TABLE I

RESULTS FROM PERMEABILIZATION EFFECT FOR VARIOUS NUMBER OF
PULSES APPLIED WHEN AN ELECTRIC FIELD OF 58 kV/Cm WAS
APPLIED AT 200-Hz PRF

Number of pulses applied	Percentage of permeabilized bacteria (mean \pm standard deviation)	Number of replicates*
5000	44.4 \pm 9.3	3
10000	69.4 \pm 12.3	6
25000	81.0 \pm 7.4	6
50000	89.3 \pm 4.7	6

* The « number of replicates » is the number of times a given condition was tested on bacteria coming from different independant bacterial cultures.

373 mixed with 600 μL of LB medium. Flow cytometry analyses
374 were performed using a BD Accuri C6 Flow Cytometer
375 (Bd Biosciences, le Pont-de-Claix, France). An excitation
376 laser of 488 nm and the FL1 bandpass filter 533/30 were
377 used to detect fluorescence of either YO-PRO-1 iodide and
378 SYTO 9 (the reason why these markers could not be used
379 simultaneously). For data processing, *E. Coli* were gated
380 and separated from debris based on FSC-A and SSC-A
381 morphological criteria. Nevertheless, a small proportion of
382 events was not SYTO 9 positive within this gating, meaning
383 that there was still debris. Thus, the specificity of the gating
384 was calculated as (6) and (7), shown at the bottom of the
385 page.

386 The specificity of the gating was evaluated for the different
387 experimental conditions (Sham or PEF exposures), and was
388 considered for further data processing. Finally, the percentage
389 of permeabilized bacteria was calculated using YO-PRO-1
390 iodide following (7).

391 VI. PRELIMINARY RESULTS

392 We assessed the ability of the subnanosecond pulses deliv-
393 ered by our system to induce electroporation on *E. Coli* DH5 α ,
394 applying trains of 5000 to 50000 pulses at a PRF of 200 Hz
395 at an electric field amplitude of 58 kV/cm (the top electric
396 field amplitude deliverable with the present arrangement). All
397 conditions tested efficiently generated electroporation of the
398 bacteria to YO-PRO-1 iodide, a fluorescent nucleic acid stain
399 and cell permeabilization marker of approximately 630 Da.
400 Moreover, under these conditions, we observed an additive
401 effect of the pulses, the percentage of permeabilized bacteria
402 increasing from 44.4 % \pm 9.3 % to 89.3 % \pm 4.7 % for 5000 to
403 50000 pulses applied, respectively (Table I). Importantly,
404 no increase of the temperature within the samples submitted to
405 PEF treatment was noticed under the conditions tested in this
406 study, in line with the estimated temperature rise presented
407 above under Section IV. Thus, the permeabilization of *E. Coli*
408 observed in response to PEF exposure performed in this study
409 cannot be attributed to thermal effects.

$$\text{Gating Specificity (GS)} = \frac{\text{number of SYTO@9 positive events}}{\text{total number of events}} \quad (6)$$

$$\% \text{ permeabilized bacteria} = \frac{\frac{\% \text{ of YO-PRO-1 positive events in sample}}{\text{GS sample}} - \frac{\% \text{ of YO-PRO-1 positive events in control}}{\text{GS control}}}{100 - \frac{\% \text{ of YO-PRO-1 positive events in control}}{\text{GS control}}} \times 100 \quad (7)$$

VII. CONCLUSION AND THE WAY AHEAD

A relatively simple arrangement for PEF processing driven by a subnanosecond pulsed power generator has been developed and tested. The preliminary results show that subnanosecond processing can be highly efficient. The way ahead will require the development of a compact, high PRF and mobile subnanosecond 0.5-MV pulsed power generator that, when coupled with a prolate reflector, will allow biomedical experimentation at (or near) a hospital.

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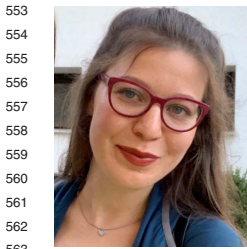
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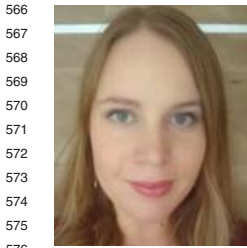
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Njomza Ibrahim (Graduate Student Member, IEEE) received the B.Sc. degree in electrical engineering from the University of Pristina, Pristina, Kosovo, in 2015, and the M.Sc. degree from the University of Pristina in 2017, combined with a one-year exchange study/research period at the Norwegian University of Science and Technology, Gjøvik, Norway. She is currently pursuing the Ph.D. degree with the Department of Electrical Engineering, Université de Pau et des Pays de l'Adour (UPPA), Pau, France.

Her research interests include high-voltage pulsed power systems and high-power microwave generation and transmission and their application in the biomedical domain.



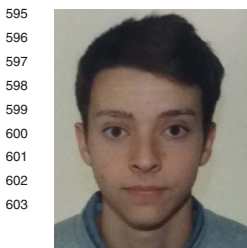
Leslie Vallet received the M.Sc. degree in chemical engineering from CPE Lyon Engineering School, Villeurbanne, France, in 2018, associated with one-year exchange study period at the Ecole Polytechnique Fédérale de Lausanne, Lausanne, Switzerland, specializing in biology. She is currently pursuing the Ph.D. degree with the METSY Unit, Gustave Roussy European Cancer Centre, Villejuif, France.

Her research interests include the interactions between biological cells and electric fields for medical application purposes.



Franck M. Andre (Member, IEEE) received the master's degree in engineering (Science for Biological and Food Industries) from the Paris Institute of Technologies AgroParisTech (ex INA P-G), Paris, France, in 2002, and the Ph.D. degree for his research performed on *in vivo* gene electrotransfer from the ABIES Doctoral School, Paris Institute of Technologies AgroParisTech, in 2006.

During his postdoc (2007–2009) at the Frank Reidy Research Center for Bioelectrics, Old Dominion University, Norfolk, VA, USA, he investigated the effects of nanosecond pulsed electric fields on cell and nuclear membrane permeabilization. He is currently a Researcher with the French National Centre for Scientific Research (CNRS), Villejuif, France. For the last few years, his research has been mainly focused on electroporation-based gene transfer and drug delivery and on the use of electric pulses to manipulate the cytosolic calcium oscillations.



Laurent Ariztia received the B.Sc. and M.Sc. degrees from the Université de Pau et des Pays de l'Adour (UPPA), Pau, France, in 2017 and 2019, respectively.

He is currently an Engineer at the SIAME Laboratory. His research interests are mainly focused on pulsed power systems, such as Marx generators, and pulse forming lines for military and civil applications.



Marc Rivaletto was born in Tarbes, France, in 1960. He graduated from the Supélec Electrical Engineer School, Gif-sur-Yvette, France, in 1984, and the Ph.D. degree in electrical engineering from Pau University, Pau, France, in 1997.

He is currently a Lecturer at Pau University and works in the SIAME Laboratory. His research interests are HPM sources, compact pulsed power systems, including pulse forming lines, compact Marx generator, and resonant transformer.



Antoine Silvestre de Ferron was born in Tarbes, France, in 1977. He received the master's degree in electrical and electronic engineering from the University of Toulouse, Toulouse, France, in 2002, and the Ph.D. degree in electrical engineering from the University of Pau, Pau, France, in 2006.

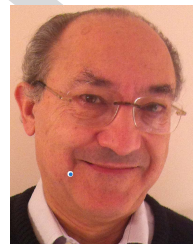
From 2006 to 2008, he was a Researcher with the Atomic Energy Commission (CEA), a French government-fund technological research organization in Le Barp, France. He is currently an Engineer with the Electrical Engineering Laboratory, University of Pau. His research interests include pulsed power generation, with military and civil applications and the high-voltage transient probes associated.



Bucur Mircea Novac (Senior Member, IEEE) received the M.Sc. and Ph.D. degrees from the University of Bucharest, Bucharest, Romania, in 1977 and 1989, respectively.

He joined Loughborough University, Loughborough, U.K., in 1998, where he is currently a Professor of Pulsed Power. He has coauthored two books on explosive pulsed power and has published more than 200 refereed papers and conference contributions. His research interests include compact and repetitive high-power systems, explosively and electromagnetically driven magnetic flux compression generators and their applications, electromagnetic launchers, ultrafast magneto-optic and electrooptic sensors, and 2-D modeling of pulsed-power systems.

Dr. Novac is a Voting Member of the Pulsed Power Science and Technology Committee in the IEEE Nuclear and Plasma Science Society. He is also a member of the International Steering Committees for both the MEGAGAUSS Conferences and the Euro-Asian Pulsed Power Conferences. He is also the Co-Chairman of the U.K. Pulsed Power Symposium. He is a fellow of the Royal Academy of Engineering, and a Chartered Engineer and a fellow of the Institution of Engineering and Technology (IET), all in U.K.



Lluís M. Mir graduated from École Normale Supérieure, Paris, France, and received the D.Sc. degree from the University of Toulouse, Toulouse, France, in 1983, and three Doctorate Honoris Causa degrees from the Universities of Buenos Aires (Argentina), Lima (Peru), and Ljubljana (Slovenia), in 2018.

As the DRCE at CNRS, he directed the Laboratory of Vectorology and Anticancer Therapies from 2010 to 2019 and the European Associated Laboratory for the applications of electric pulses in biology and medicine from 2011 to 2018. He published 238 peer-reviewed articles and 25 book chapters (H index = 70, WoS).

Dr. Mir is a fellow of the American Institute for Medical and Biological Engineering, the European Academy of Tumor Immunology, and the Radio-Science International Union (URSI). He won several awards, including the URSI's 2017 Balthasar van der Pol Gold Medal. He is the present President of the International Society for the Electroporation Based Treatments and Therapies.



Laurent Pécastaing (Senior Member, IEEE) received the Ph.D. and Research Directorship Habilitation degrees in electrical engineering from the Université de Pau et des Pays de l'Adour (UPPA), Pau, France, in 2001 and 2010, respectively.

He is currently a Full Professor in pulsed power with the Laboratoire SIAME, UPPA. He is the Head of the High Voltage Processes Team, Laboratoire SIAME, and he is also the Director of a Common Laboratory, CEA, Paris, France. His current research interests include high-power microwave sources, compact pulsed power systems, and ultrafast transient probes.

Dr. Pécastaing is the Chairman of the next EAPPC/BEAMS/MEGAGAUSS Conference to be held in France in 2021. He is also a member of the International Steering Committees for both the BEAMS Conferences and the Euro-Asian Pulsed Power Conferences.